

SEGMENTATION OF LIVER ULTRASOUND IMAGES USING GAUSSIAN KERNEL FUZZY CLUSTERING AND REGION BASED ACTIVE CONTOUR MODEL

Jasdeep Kaur¹, Bhwana Utreja²

¹Department of ECE Punjabi University, Patiala Punjab, India

²Assistant Professor, Department of ECE Punjabi University, Patiala, Punjab, India

Abstract

Since liver disease is the 6th most regular threatening tumor on the planet and the third most normal reason for malignancy related deaths around the world. Subsequently, it is imperative to create a typical standard instrument, for detection of tumors which can perform determination with same ground criteria consistently all over the world. In this work, we have introduced a noble method for detection of tumor in liver ultrasound images. In existed work, little work has been found on liver segmentation. Then active contour segmentation has been carried out to segment the tumor region in the image. Experimental results show approx. 95% accuracy rates on the dataset collected for evaluating the algorithm

1. INTRODUCTION

Segmentation is the procedure of sub-isolating a picture into its constituent locales or articles. Segmentation ought to stop when the objects of enthusiasm for the application have been segregated. Presentation Liver malignancy is the third most regular reason for death from growth overall [1], and liver is the most well-known metastatic spread locales of tumors after the lymph hubs, which have been found in 30–70% of patients who are passing on of disease [2]. However, precise and dependable liver division keeps on being a testing undertaking particularly for sick livers in light of the distortion of the liver shape brought on by substantial tumors, the multifaceted nature of the infected liver pathologies, the variability of picture nearness of various hepatic illnesses, (for example, hypo thick or hyper thick injuries), and the fluffy limits amongst liver and the neighboring organs, (for example, heart and stomach). Along these lines, liver division draws in persistently specialists considerations in medicinal imaging and representation group. Picture division is the division of a picture into locales or classes, which compare to various questions or parts of items. There have been Numerous division techniques proposed for different applications, e.g. PC vision [3], object acknowledgment [4–6], and restorative imaging.

1.1 Segmentation of Liver Ultrasound Images

The liver is the biggest organ in the body, and it includes all the biochemical pathways that capacity in permitting development, battling malady, supplying supplements, giving vitality, and supporting multiplication. The picture quality from various modalities changes as far as sign to-commotion proportion, movement curios, and so forth. There are a few reports on the division of the stomach organs on CT pictures by utilizing a thresholding strategy, probability capacity, or hepatic vessels [4–6]. In any case, numerous reports address just strategies including division

of the ordinary liver tissues and these procedures can't ordinarily be utilized for separating the anomalous liver districts. Bae et al. [7] utilized a thresholding technique to section the liver in living contributor stomach CT pictures. In this technique, a dark level edge was resolved from the histogram; along these lines, the division would be influenced by the nearness of substantial hepatic tumors with various force inside the liver or other associated organs and by the tissues that had covering thickness

1.2 Proposed Work

We proposed a half breed strategy for division of abandoned area in liver US in view of the blend of the wavelets, round Hough change, form division, fluffy bunching and morphological handling and so on wavelet changes can be utilized as a part of assignments extending from edge identification to picture smoothing. Because they give critical understanding into both a picture's spatial and recurrence attributes, wavelets can likewise be utilized as a part of uses in which Fourier strategies are not appropriate, similar to dynamic picture recreation. The following is a flowchart for the procedure

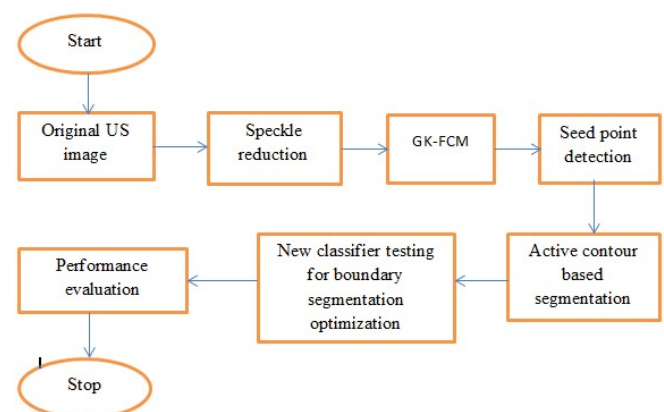


Fig 1.1 Flowchart of the proposed analysis

The different strides for proposed calculation are given beneath:

1. Load Tumor picture
 2. Use wavedec2 capacity for disintegration
 3. Use wavedec2 capacity for decay
- Extricate all level estimation and point of interest coefficients.
4. Show deterioration up to multi levels utilizing pyramid approach.
 5. Assess versatile limit
 6. Apply wdencomp for denoising utilizing "lvd" parameter for limit.
 7. Contrast-restricted versatile histogram balance (CLAHE).
 8. Apply band restricted 2-D Gaussian channel
 9. Apply roundabout Hough change to get roundabout blob in tumor area.
 10. Apply GKFCM to get two classes of pixels and actualize 2-D Gaussian channel for separating high and low power areas
 11. Apply Region Based Active Contour Segmentation utilizing seed point from circle identified
 12. Measure execution utilizing affectability and specificity values

Step 1) Speckle Noise Reduction by Wavelet Transforms

Step one includes the disintegration of picture utilizing distinctive wavelets at various levels. Diverse wavelets work in various way. For instance Haar, waveform takes a pixel pair at once and discovers estimation and point of interest coefficients for every pair. As the level going to expand the quantity of pixel sets stayed for disintegration will diminish by variable. Debauchees work in same path as haar with the exception of the window utilized for ascertaining coefficients is expanded by sort utilized. The following are the outcomes after deterioration of Haar at level four. There are two techniques for picking edge. One is worldwide and other is versatile or variable.

In this, remaking has been completed utilizing thresholded point by point coefficients and estimation coefficients. We connected hard and delicate thresholding both for worldwide and in addition versatile. The following is the assume that portrays yields when hard and delicate thresholding are connected on a sign.

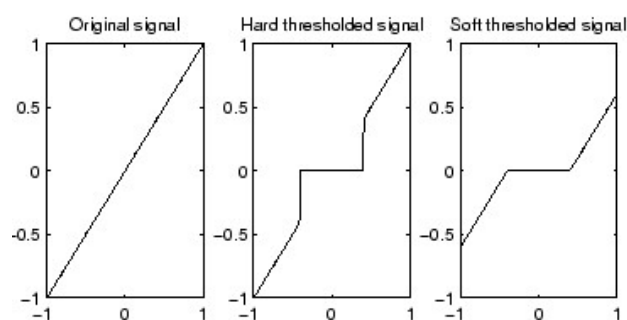


Fig 1.2: Orginal signal with hard and soft thresholding.

Below are results of our work after denoising step.



Fig 1.3: original image

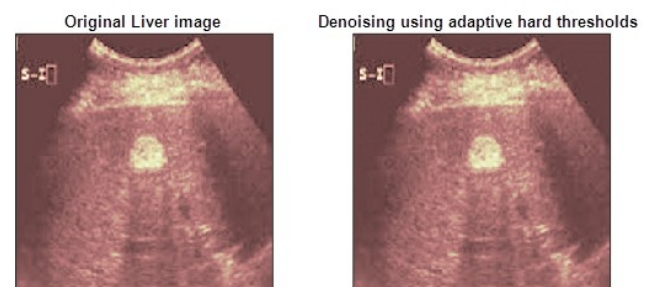


Fig 1.4: Denoised image using variable hard thresholding.

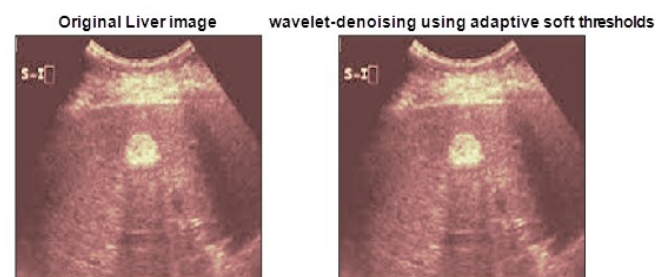


Fig1.5: Denoised image using variable soft thresholding.

Area channel is basically a spatially changing channel that naturally modifies itself to the neighborhood flag and commotion structure. One of the key elements of the wavelet change is that it gives data about how the recurrence substances of the sign shift after some time.

In discrete wavelet transform (DWT) investigation, the resultant coefficients are gone through an edge testing, and the coefficients that are littler than a specific worth, are expelled. At that point, the resultant coefficients are utilized to remake the sign. The utilization of this strategy results in the expulsion of commotion without much loss of points of interest. The DWT strategy depends on the suspicion that the adequacy of spectra of sign is not quite the same as that of the commotion spectra. This permits thresholding and contracting of the abundancy of coefficients to separate flags or evacuate commotion. In the analysis, delicate thresholding has been utilized over hard thresholding in light of the fact that it gives all the more outwardly lovely pictures contrasted and those hard thresholding.

Step 2) Contrast Enhancement by Contrast-Limited Adaptive Histogram Equalization

Contrast-limited adaptive histogram equalization image



Fig 1.6: Image showing output after Contrast-limited adaptive histogram equalization

Contrast Limited AHE (CLAHE) varies from normal versatile histogram balance in its differentiation constraining. This element can likewise be connected to worldwide histogram evening out, offering ascend to Contrast Limited Histogram Equalization (CLHE), which is once in a while utilized as a part of practice. On account of CLAHE, the difference constraining system must be connected for every area from which a change capacity is inferred.

Step 3) Circular Blob Detection Inside Tumor Region by Circular Hough Transforms

Circular blob found in infected region

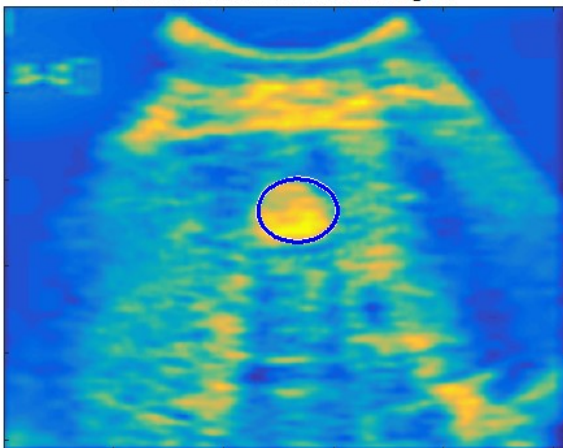


Fig 1.7: Circular blob detected in tumor region

Rather than lines, Circular, curved, allegorical shapes can likewise be distinguished by utilizing HT. For round shape, three variables are x and y directions of the inside and the span. We require three dimensional explanation focuses for sparing these three variables. Like straight line, round shape identification in light of HT goes for the voting. Curved shape is having five variables: x and y directions of the middle, semi-major-axis (a), semi-minor-axis (b) and point

theta amongst semi-major-axis and x pivot. The parameter space must group around the parameter values which compare to that shape. Nearby data innate in the purposes of the shape, for example, contiguousness is lost end purposes of circle circular segments and line fragments must be resolved in a consequent stride. Computational heap of the strategy increments quickly with the quantity of parameters which characterize the recognized shape. We chose initial three most conspicuous circles from which we utilized that circle which has high normal force.

Step 4) Final Segmentation of Infected Liver Using Contour Segmentation

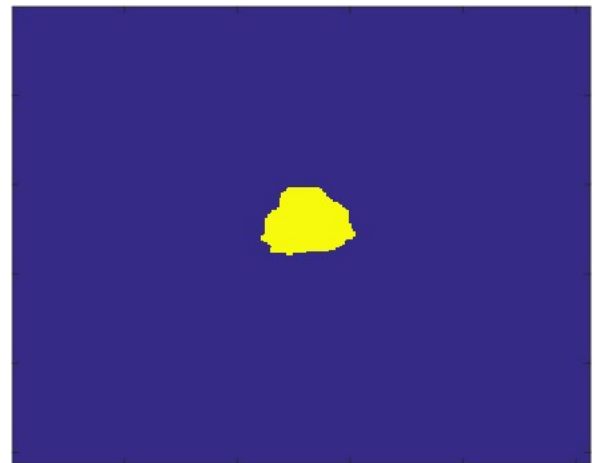


Fig 1.8: Final segmented region evaluated in high intensity pixels .

Performance Parameters

True Positive (TP)

It signifies the pixels that get to be accessible in both the portioned area produced by manual and mechanized division strategy. The TP is characterized as,

$$TP = \frac{|S_M \cap S_T|}{S_M}$$

Where SM alludes to physically segmented ground truth binary cover.

ST demonstrates the area segmented by the electronic test techniques.

In the event that the TP gets higher qualities, it implies the all the more covering zone between ground truth and fragmented area.

False Positive (FP)

It means the pixels that get to be unmistakable in the segmented locale created by test technique, however it doesn't showing up the ground truth parallel veil. At the point when the FP takes lower esteem less off base locales are removed by the test strategy. The FP proportion is given as,

$$FP = \frac{|S_M \cup S_T - S_M|}{|S_M|}$$

Sensitivity

Sensitivity is a factual measure that characterizes the extent of genuine positive subjects with the ailment in an aggregate gathering of subjects with the infection (TP/TP+FN).

It gives the likelihood of getting a positive test result in subjects having contaminated skin. Thus it identifies with the capability of a test to perceive subjects with the sickness [8].

Specificity

This measure of precision of a symptomatic test is correlative to affectability. It is characterized as the extent of subjects without the contaminated pixels with negative test result to the aggregate number of subjects without ailment

(TN/TN+FP). In other words, specificity speaks to the likelihood of a negative test result in a subject without the ailment. Along these lines, it depicts the test capacity to perceive subjects without the infection [8].

Accuracy (ACC) demonstrates the extent of the pixels contained inside the accurately extricated district got by the test technique out of all pixels of the physically portrayed area. The segmentation accuracy is characterized as,



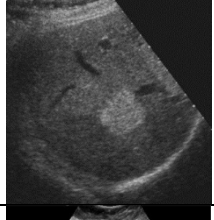

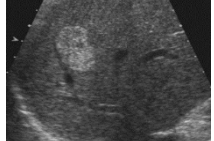
$$ACC = \frac{TP + TN}{TP + FP + TN + FN}$$

2. RESULTS

The results in terms of specificity are shown below

Below is the table showing different parameters for input images:

Table 5.1: Table one showing sensitivity and specificity parameters

Image NO.	True +VE	False -VE	True -VE	False +VE	Sensitivity	Specificity	Accuracy	Images
Image1	1124	27	64156	229	0.9765	0.9964	0.9864	
Image2	1540	80	63782	134	0.9506	0.9979	0.9742	
Image3	2156	216	62926	238	0.9089	0.9962	0.9525	
Image4	2114	6	62538	878	0.9971	0.9861	0.9916	
Image5	1982	30	62542	982	0.9850	0.9845	0.9847	

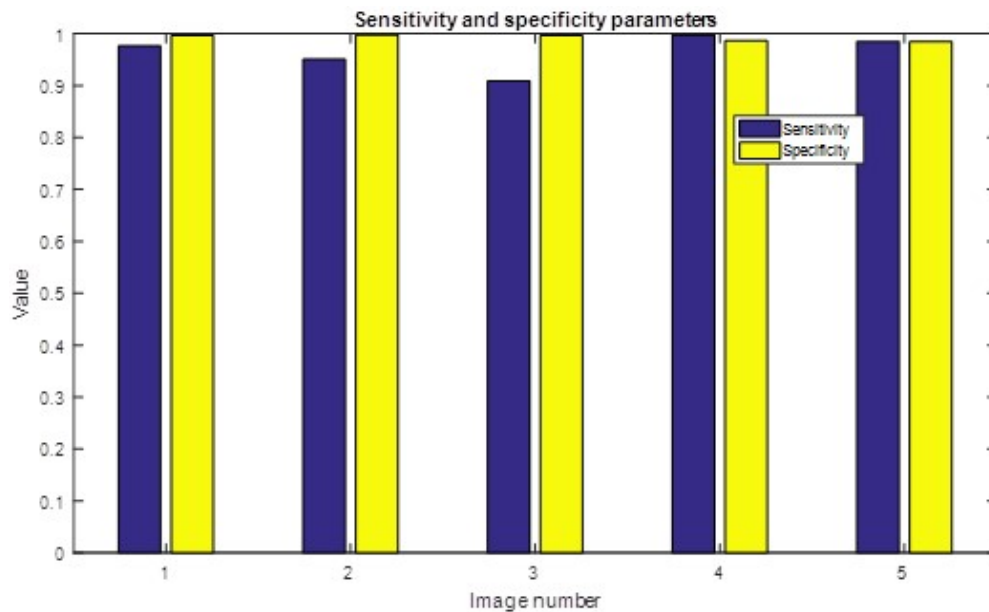


Fig 1.9: Bar graphs for sensitivity and specificity values

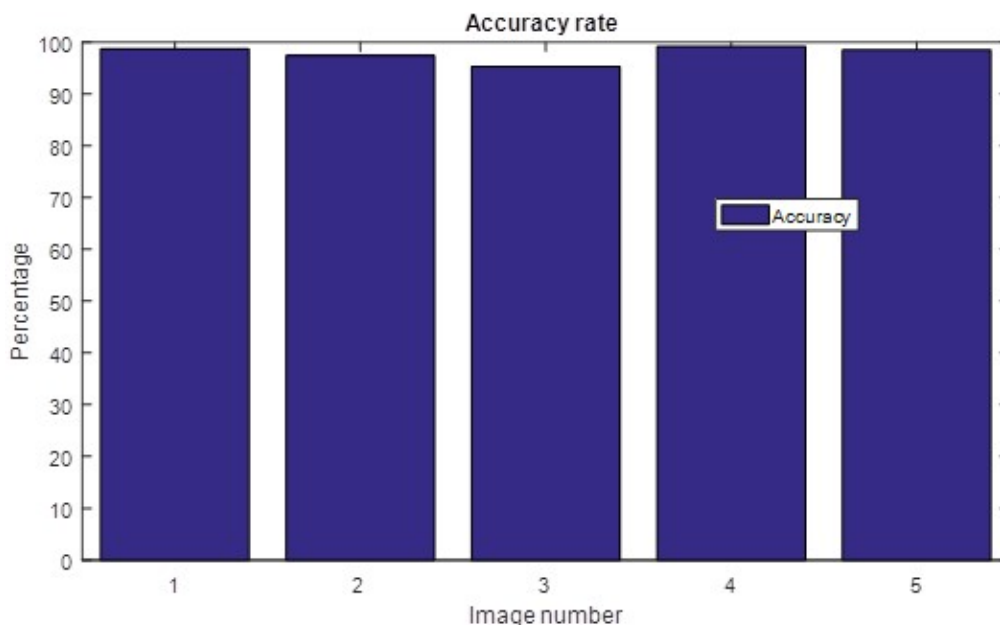


Fig: 1.10 Accuracy

From the outcomes appeared above it has been found that the proposed calculation has high affectability and specificity values. In a large portion of the cases these worth are above 90 %, which comes in great class of the outcomes. We have given results to few pictures as depiction yet we attempted the calculation on number of pictures.

3. CONCLUSION

In this work, we propose a picture improvement and segmentation strategy utilizing wavelet transform, round Hough transform and shape division so as to give a valuable rule to applying division of tainted locale in restorative field. The recreation tests have been done utilizing pictures with various organs, commotion levels, and transducer recurrence. In this first of debauchees wavelet has been connected to evacuate spot clamor in the picture, After that

Contrast-constrained versatile histogram equalization has been connected for difference change. At that point round Hough transform has been utilized to get the roundabout blob in the contaminated tumor area. At last Chan-Vese form division has been connected utilizing round blob area to section out tainted locale in the picture. Proposed strategy gives magnificent on round and curved tumors. In future work, same calculation can be enhanced to get consider irregular shape tumors in Liver US pictures.

REFERENCES

- [1]. G Xiao, M Brady, JA Noble, and Y Zhang, Segmentation of ultrasound B-mode images with intensity inhomogeneity correction, *IEEE Trans. On Med Imag*, Vol. 21, pp. 48-57, 2002.

- [2]. Vibhhrimali, R.S. Anand and Vinod Kumar, Comparing the Performance of Ultrasonic Liver Image Enhancement Techniques: A Preference Study , IETE Journal of Research, Vol. 56, Issue 1, Jan-Feb 2010.
- [3]. Wan Mahani Hafizah, Eko Supriyanto, —Comparative Evaluation of Ultrasound Kidney Image Enhancement Techniques, International Journal of Computer Applications (0975 – 8887) Volume 21– No.7, May 2011.
- [4]. Y Yu, and S T Acton, Speckle Reducing Anisotropic Diffusion, *IEEE Trans. on Image Process*, Vol. 11, pp. 1260-70, 2002.
- [5]. S W Smith, and H Lopez, A contrast-detail analysis of diagnostic ultrasound imaging, *Med. Phy*, Vol. 9, pp. 4-12, 1982.
- [6]. Smriti Sahu¹, Maheedhar Dubey, Mohammad Imroze Khan, “Liver Ultrasound Image Analysis using Enhancement Techniques”, International Journal of Advanced Computer Research , Vol. 2 , No. 2, pp. 125-29 , 2012.
- [7]. Alka Vishw, Vishakha Goya, “An Improved Threshold Estimation Technique for Ultrasound Image Denoising” , International Journal of Advanced Research in Computer Science and Software Engineering, Vol. 3 , pp. 96-102 , 2013.
- [8]. Simundic A. Measures of diagnostic accuracy: basic definitions. *Med Biol Sci* 2008; 22(4):61-5.