

# PERFORMANCE COMPARISON OF NOISE REDUCTION IN MAMMOGRAM IMAGES

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## Abstract

Noise level present in mammogram images highly affects the image analysis and accuracy of classification. Hence removing noise present in mammogram images is an important task. Noise present in the medical images depends on imaging modalities. The dominant noise present in mammogram images are quantum noise. The objective of this work is to study the various filters such as mean, median and wiener filter with different window size using standard benchmark (Digital Database for Screening Mammography) DDSM dataset. Higher the value of the (Peak Signal to Noise Ratio) PSNR, better the image quality of the restored image. The restored image quality of various filters was evaluated with PSNR value. We obtained, the wiener filter with window size 3x3 gives better result for noise reduction in mammogram images.

**Key Words:** Mammogram, Quantum Noise, Mean Filter, Median Filter, Wiener Filter, DDSM and PSNR

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## 1. INTRODUCTION

The imaging noises reduce the quality of the acquired medical images. The noise present in the images depends on the imaging modalities. In X-ray mammogram, the dominant noise is quantum noise. Images cannot be used as they are, because they contain some noise. Hence removal of noise that might result while scanning is important to get accurate information. In the noise removal process, filtering techniques are used. In this paper we are analyzing different filtering technique to find the efficient one in the process of Digital mammogram images enhancement.

## 2. MAMMOGRAM IMAGES

Mammography has been proved to be the primary radiologic procedure for the early detection of breast cancer. The indicator of breast cancer in a mammogram is the presence of a tumor mass. DDSM database images are used for the experimental study. Quantum noise are the dominant in mammogram.

## 3. QUANTUM NOISE

Noise level present in the images highly affect the quality and accuracy of classification when working with Mammographic images. The dominant noise present in the mammographic images are quantum noise. Quantum noise occurs inherently in low – dose X –ray imaging due to the very low X – ray quantum counts.

## 4. DENOISING TECHNIQUES

Filtering technique are used to denoise the image. In this paper we describe several filtering methods such as mean, median, wiener filter to reduce the quantum noise present in mammogram images.

### 4.1 Mean Filter

Let  $S_{xy}$  represent the set of coordinates in the window  $m \times n$ , centered at point  $(x, y)$ . The mean filter computes the average of value of the corrupted image  $g(x, y)$  in the area defined by  $S_{xy}$

$$f(x, y) = \frac{1}{mn} \sum_{(s,t) \in S_{xy}} g(s, t)$$

where  $f(x, y)$  Value of restored image at point  $(x, y)$

### 4.2 Median Filter

Here the magnitude of all the vectors is taken with in a mask and arranged according to the magnitude. The median magnitude pixel is then used to replace the pixel studied. This filter is given by

$$\text{Median filter } (X_1, \dots, X_n) = \text{median } (\Pi_{x_1} \Pi_2 \dots \Pi_{x_N} \Pi_2)$$

### 4.3 Wiener Filter

The following are the characteristics of the wiener filter.

- Signal and noise are stationary. The linear random proces are made with known spectral characteristics.
- Requirement: Filter must be physically realizable.
- Performance criteria:

$$G(u, v) = \frac{H^*(u, v)p_s(u, v)}{H(u, v)I_2p_s(u, v) + p_n(u, v)}$$

Where  $H(u, v)$  is the Degradation Function

$H^*(u, v)$  is the complex conjugate of degradation function

$P_n(u,v)$  is the Power spectral density of noise

$P_s(u,v)$  is the Power spectral density of undegraded image.

### 5. EXPERIMENTAL RESULTS

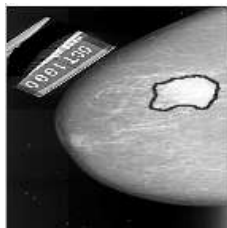
The images for this study were obtained from DDSM Database. The performance of the proposed filters is uniformly by resizing all the images to 256x256 pixels. To evaluate the performance of the various filter, we used PSNR image quality performance metric. The PSNR value of the denoised image is calculated using the following formula..

$$PSNR = 10 \log_{10} \frac{\sum I \sum i 255^2}{\sum I \sum i (S_{i,j} - K_{i,j})^2} db$$

Where  $S_{i,j}$  is the original image  
 $K_{i,j}$  is the restored image.

Following figure1 shows the input and output image for image 01

DDSM IMAGE 01



Input image

MEAN FILTER



MEDIAN FILTER



WIENER FILTER



Output image of various filters for Image 01 (window size 3 x 3)

Fig-1: Input and Output Image for Image 01

Table-1: PSNR value of the images studied with different window size and result

DDSM Image	Window Size	Mean Filter	Median Filter	Wiener Filter
Image 01	3x3	25.08	30.69	<b>35.69</b>
	5x5	21.68	23.94	32.40
	7x7	20.16	22.51	30.78
Image 02	3x3	27.74	31.80	<b>35.92</b>
	5x5	23.87	26.62	32.35
	7x7	21.91	23.93	30.73
Image 03	3x3	27.89	33.50	<b>35.88</b>
	5x5	24.17	28.30	32.57
	7x7	22.18	22.60	31.08
Image 04	3x3	27.31	31.54	<b>36.94</b>
	5x5	23.31	24.85	33.08
	7x7	21.24	20.66	31.47
Image 05	3x3	25.77	28.45	<b>37.36</b>
	5x5	22.70	25.19	33.72
	7x7	21.08	23.67	31.91

Following figure2 shows the comparison of PSNR value for image 01 with different window

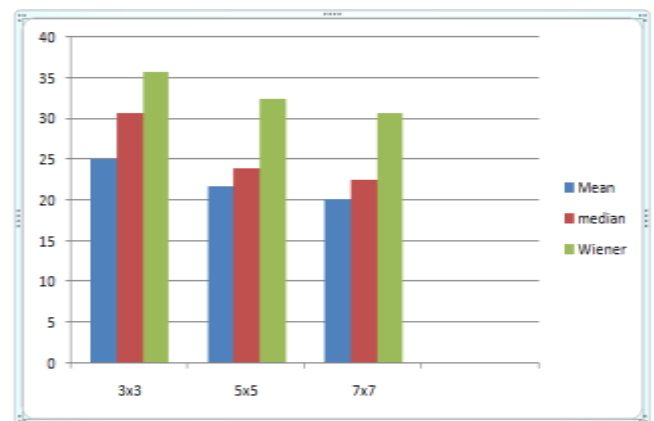


Fig-2: Comparison of PSNR value for Image 01 with Different Window

### 6. CONCLUSION

In this paper, we have presented the performance comparison of mammogram images with different window size using mean, median, wiener filter. The performances are analyzed according to PSNR value. We obtained, the wiener filter with window size 3x3 gives better result for noise reduction in mammogram images. For future work we would like develop a noise reduction method by combining filters, and also to compare with various image quality evaluation metrics.

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