

TRANSFER ENTROPY ESTIMATION SUPPLEMENTS TIME-DOMAIN BEAT-TO-BEAT BAROREFLEX SENSITIVITY INDEX UNDER POSTURAL STRESS

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Abstract

Baroreflex mechanism plays a vital role in cardiovascular regulation by contributing in sympathetic-vagal imbalance triggered by baroreceptor reflex. This study estimates BRS (Baroreflex Sensitivity) index from beat-to-beat systolic blood pressure (SBP) and RR interval (RRi) series using time-domain windowed cross-correlation method. This index is supplemented by an information domain technique called Transfer Entropy (TE) is applied to decipher the directional coupling between SBP and RRi series. The study is performed on EUROBAVAR data. The results show that BRS index calculated is large (1.157 ± 0.533) in supine position which supplemented by TE (SBP-RR) of (0.129 ± 0.09) as compared to standing position for which BRS index is (0.866 ± 0.472) and a TE (SBP-RR) of (0.04 ± 0.03) for EUROBAVAR data with a p -value < 0.05 . Also, it is found that both the TE indices i.e. from SBP to RR and from RR to SBP show correlated results with the time domain BRS index in both supine and standing positions. Further, the cases with possible BRS failure are having very small values of BRS index, which are not assigned any value by prevalent methods. This shift is absent in BRS failure patients which is supplanted by TE (RR-SBP) sharing more information bits than TE (SBP-RR). Further, it is observed that patients having baroreflex impairment show reversal of information flow which is indicated by a larger TE (RR-SBP) index as compare to TE (SBP-RR) index. Time domain BRS index lacks directional information which is provided by TE and hence this supplemental information gives better interpretation of BRS index especially in patients having suppressed baroreflex.

Index Terms: Baroreflex sensitivity, Directional coupling, Cross-correlation, and Transfer entropy

1. INTRODUCTION

Baroreflex modulates both cardiac parasympathetic and sympathetic outflow to the sinus node in the heart. Quantification of this baroreflex control can be done by an index known as Baroreflex Sensitivity (BRS) which depends on the rate of change of heart rate corresponding to rate of change of systolic pressure [1]. Cardiac baroreflex sensitivity index is known to have been influenced by certain cardiac autonomic function tests viz. supine-to-standing test, Valsalva manoeuvre, deep breathing, cold pressor test and handgrip test [2,3].

In the Task Force paper [4], it has been quoted that unlike heart rate variability (HRV), BRS index is able to distinguish between post myocardial infarction cardiac arrest (MI-CA) survivors from other post MI patients. BRS index is also able to assess autonomic dysfunction of diabetic patients [5]. Over the last two decades, BRS index has emerged as a great prognostic indicator of wide range of cardiovascular diseases [6,7]. Both invasive and non-invasive methods have been developed over a period of time to analyze baroreflex sensitivity. The invasive methods use external stimulus such as drugs to vary the blood pressure thereby activating the baroreflex. Recent methods use non-invasive means of

evaluating BRS and are based on spontaneous beat-to-beat measurement of both blood pressure and heart rate. Sequence method and cross correlation method are among the popular time domain methods. Frequency domain methods include parametric and non-parametric spectral estimation to estimate low frequency (LF) and high frequency (HF) gain [8]. Some studies have also taken into account the phase or time-delays between beat-to-beat systolic pressure and RR intervals series to estimate BRS [9]. Directional coupling information needs to be quantified to provide a more complete estimation of BRS index which cannot be calculated using linear time domain index. Some earlier studies [9] have utilized mutual information and time delayed mutual information to calculate amount information exchanged between the two signals which are generated by a same system. In this paper, a BRS index obtained using beat-to-beat cross-correlation analysis of SBP and RRi series supplemented by calculating the directional coupling index using information theory based Transfer Entropy method is presented.

2. DATA SAMPLES AND PRE-PROCESSING

21 subjects from EUROBAVAR dataset (4 males and 17 females) aged 20 to 68 years (38 ± 14.7 , mean \pm SD) are taken for BRS estimation. In the EUROBAVAR dataset there are 4 healthy volunteers, 8 outpatients, 3 hypertension patients, 2 hypercholesterolemia patients, 1 diabetic without neuropathy, 1 diabetic with neuropathy (BRS failure), 1 heart transplant patient (BRS failure) and 1 pregnant woman.

2.1 Data Pre-processing

Systolic blood pressure (SBP) values and R-peaks are detected using an algorithm based on empirical mode decomposition (EMD). The EMD method decomposes the ECG signal and Blood Pressure (BP) signal into a set of oscillatory components called intrinsic mode functions (IMFs). This is a data driven method unlike wavelet transformation which decomposes the input signal based on a pre-defined kernel [11]. Ectopic beats were manually removed from the EUROBAVAR as well as from the recorded data. From the detected peaks of both ECG and BP signal, time series of RR intervals (RRi) and SBP values are formed. The SBP and RRi series for n number of samples are normalized by subtracting and then dividing by the mean.

For TE implementation an increase in RR interval and SBP value is taken as "1" and a decrease in subsequent values is taken as "0". In this way a series of binary symbols is generated which is used to calculate the transfer entropy from SBP to RR and from RR to SBP.

3. METHODS

Both time domain and information theory based methods are applied to quantify the mutual coupling between SBP and RRi time series. Time domain method is a linear technique which provides BRS index but does not provide bi-directional interaction between SBP and RRi series whereas information theory based TE method quantify directional coupling between the two series under consideration. A detailed explanation these techniques are as follows.

3.1 Time domain cross-correlation method

Beat-to-beat SBP and RRI series are considered for each subject. Beat events are synchronized according to RR intervals. A 10 beat sliding window is used to find the correlation between each SBP value and RR interval. To start with, SBP values corresponding to first 10 beats were considered and their cross correlation with first 10 RRI values is performed using the following equation [1]:

$$\rho = \frac{N \sum_{i=1}^N RRI_n(i) \cdot SBP_n(i) - \sum_{i=1}^N RRI_n(i) \sum_{i=1}^N SBP_n(i)}{\sqrt{\left\{ N \sum_{i=1}^N (RRI_n(i))^2 \right\} - \left\{ \left(\sum_{i=1}^N RRI_n(i) \right)^2 \right\}} \sqrt{\left\{ N \sum_{i=1}^N (SBP_n(i))^2 \right\} - \left\{ \left(\sum_{i=1}^N SBP_n(i) \right)^2 \right\}}}$$

$$\dots(1)$$

This first calculation of cross-correlation corresponds to delay of zero beat. The next calculation is carried out on the same 10 SBP values and the interval values shifted by 1 beat. (2nd to 11th beat). The window is shifted by one beat sample till 15th RRI value and the cross-correlation is estimated for the same 10 SBP values and the shifted RRI values at each window slide. The maximum of the cross-correlation value is selected out of these 6 cross-correlation values. Regression slope is estimated between the SBP and RRI values corresponding to the maximum cross-correlation value according to the following equation [1]:

$$r = \frac{N \sum_{i=1}^N RRI_n(i) \cdot SBP_n(i) - \sum_{i=1}^N RRI_n(i) \sum_{i=1}^N SBP_n(i)}{\sqrt{\left\{ N \sum_{i=1}^N (RRI_n(i))^2 \right\} - \left\{ \left(\sum_{i=1}^N RRI_n(i) \right)^2 \right\}} \sqrt{\left\{ N \sum_{i=1}^N (SBP_n(i))^2 \right\} - \left\{ \left(\sum_{i=1}^N SBP_n(i) \right)^2 \right\}}} \quad (2)$$

This regression slope is taken as BRS index if its value is positive otherwise the corresponding segment is not counted towards estimation of BRS. The average regression slope is calculated and taken as an index of BRS. SBP and RRI values are also influenced by factors other than BRS. To account for this, the accepted regression slope is divided by the correlation coefficient to get an index called non-BRS index.

3.2 Information theory based Transfer Entropy

Estimation

TE has been established as a powerful tool for detecting the transfer of information between two joint processes [11]. TE has a solid foundation in the information theory and it naturally incorporates directional and dynamical information as it is different when computed over two causal directions [11]. TE from a process j to a process i is given by the following equations:

$$T_{j \rightarrow i} = \sum_{x_{n+1}, x_n, y_n} p(x_{n+1}, x_n, y_n) \log \frac{p(x_{n+1}, x_n, y_n) \cdot p(x_n)}{p(x_n, y_n) \cdot p(x_{n+1}, x_n)}$$

$$T_{i \rightarrow j} = \sum_{y_{n+1}, x_n, y_n} p(y_{n+1}, x_n, y_n) \log \frac{p(y_{n+1}, x_n, y_n) \cdot p(y_n)}{p(x_n, y_n) \cdot p(y_{n+1}, y_n)}$$

$$\dots(3)$$

Where x and y represents symbolic RRi and SBP series respectively. p(x), p(y) are the individual probabilities and p(x,y) and p(y,x) are the joint probabilities.

4. RESULTS AND DISCUSSIONS

4.1 Cross-correlation BRS index (xBRS)

This method provides BRS estimates for all subjects of EUROBAVAR dataset and laboratory recorded data. Table 1 provides the mean and standard deviation of the BRS estimates. It is evident that supine BRS values are greater than

standing BRS values. This is true for EUROBAVAR as well as data recorded under laboratory conditions.

4.2 Transfer Entropy Index

Table 1 also shows the TE index calculated from SBP to RR and vice-versa. These two indices convey the directional coupling information between the two time series.

Table-1: BRS index and TE index of healthy subjects

Position		Coupling Indices (Healthy)		
Supine		<i>Time-domain x-BRS index</i>	<i>TE index (SBP-RR)</i>	<i>TE index (RR-SBP)</i>
	Mean	1.157	0.13	0.11
	SD	0.533	0.09	0.09
Standing	Mean	0.866	0.05	0.04
	SD	0.472	0.03	0.03

Table 2 provides the BRS index for baro-reflex impaired patients B005 and B010 in both positions. The low values of BRS index confirm this impairment. Directional coupling which is indicated by the two transfer entropy measures also show a certain decrease in coupling as indicated by the decreased TE indices from supine to standing position in healthy subjects.

Table-2: BRS index and TE index of patients with depressed BRS

Position		Coupling Indices (Patients with depressed BRS)		
Supine		<i>Time-domain x-BRS index</i>	<i>TE index (SBP-RR)</i>	<i>TE index (RR-SBP)</i>
	Mean	0.21	0.017	0.073
	SD	0.02	0.01	0.03
Standing	Mean	0.13	0.006	0.008
	SD	0.19	0.13	0.01

The results do indicate a correlation of directional coupling indices with the time domain x-BRS index obtained from windowed cross-correlation method for both supine and standing positions.

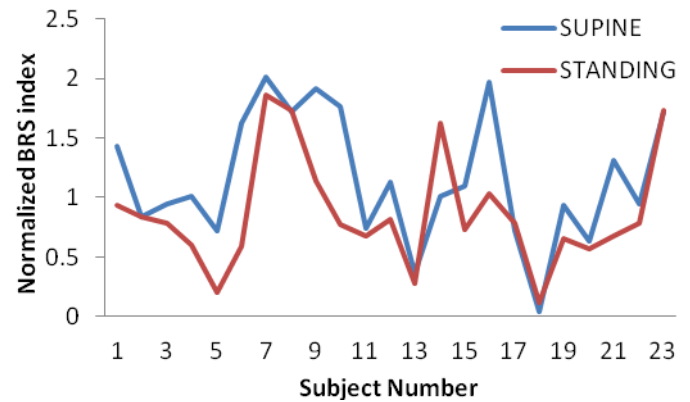


Chart -1: BRS index of all the subjects

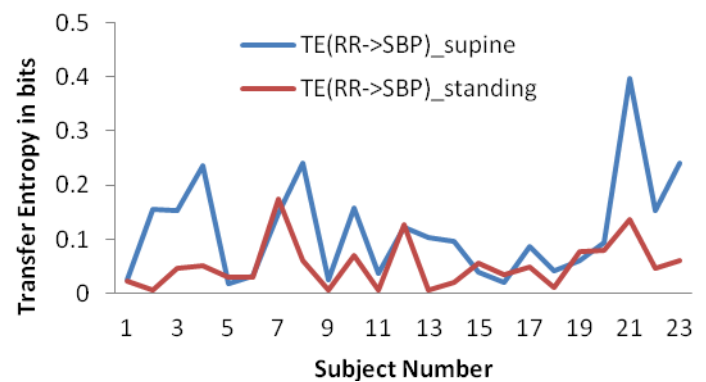


Chart -2: TE (RR-SBP) for all subjects

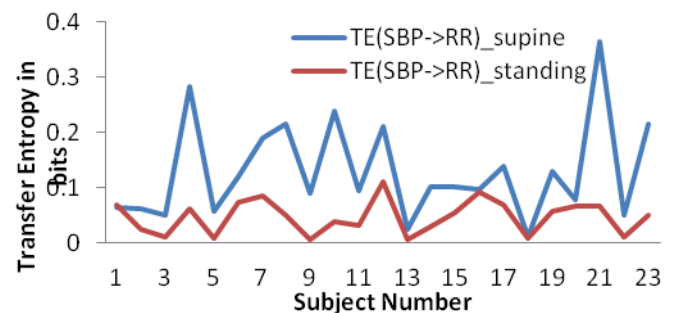


Chart -3: TE (SBP-RR) for all subjects

Chart 1, 2 and 3 show that there is a decrease in BRS as well as the coupling indices from supine to standing in most of the subjects. Since the time domain x-BRS index does not provide any directional coupling information, the transfer entropy indices supplement this information. It is worth noting that for healthy subjects in which BRS is intact the TE index from SBP to RR is greater than that of RR to SBP which shows the actual baroreflex action i.e change in SBP leads to change in RR interval. This reverses in case of patients with depressed BRS.

4.3 Significance of difference between lying and standing positions

The cross correlation BRS index and TE indices calculated by above methods differ significantly for both lying and standing positions and was evaluated using chi-square test with a p-value of 0.004.

The results also showed significant differences for delay parameter with a p-value less than 0.05. The precision in standing as well as lying position was almost same. Though the magnitudes of pressure values as well as the interval time change with a change in position the sensitivity of BRS index and TE estimation remained almost same

CONCLUSIONS

Time domain BRS index gives incomplete information and lacks interpretation in diverse patho-physiological cases since it lacks directional coupling information and its linear nature is unable to track non-linear and non-stationary fluctuations that normally occur in complex physiological signals. Transfer entropy index provides directional coupling information between SBP and RR intervals and hence supplements the BRS index obtained from traditional time domain method. The results clearly show that there is a tendency to reverse the direction of information flow in case of conditions such as heart transplantation and diabetic neuropathic conditions in which depressed BRS is recorded. Future work should concentrate on more detailed analysis based on the techniques adopted from information theory.

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